

Modelling of a lens system for the optical beam focusing of diode laser bars with high fill factor for optoacoustic applications

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Abstract

A customized optical system composed of collimating and focusing lenses is proposed to achieve the beam focusing of high-brightness diode laser bars with high fill factor for optoacoustic applications. Through an optimized design, the beam of a 940-nm diode laser bar is first collimated and symmetrized between the fast and slow axes, and then is reduced in size into a square beam (~ $3.7 \text{ mm x } 3.7 \text{ mm at } 1/e^2$ of the peak) with intensity of ~ 3.2 kW/cm^2 . In an optoacoustic environment, the optical spot achieved can illuminate a small region of tissue at high intensity to achieve in-depth imaging with high resolution.

Keywords: Diode laser bars, Laser beam shaping, Microlenses, Optoacoustics.

1. Introduction

High-power diode laser bars (DLBs) and stacks (DLSs) are extensively used in several applications, such as metal welding and soldering [1], surface treatments [2], solar cells fabrication [3], laser surgery [4], molecular and atomic spectroscopy, and military defense [5]. Recently, DLSs at 808 nm have been proposed also for optoacoustic applications [6]. These devices can provide very high values of optical peak power (from hundreds of W to several kW), but they suffer from high divergence of the propagated beam [2] that requires additional optical elements for beam shaping [7]. Industrial applications already have solutions for beam shaping of DLBs and DLSs with fill factor up to 50 % (the fill factor is the ratio between the emitter width and the emitter pitch and is expressed in percentile). Their brightness increases with the fill factor, but their beam gets more complex to handle due to the short distance between emitters. Unfortunately, the market does not offer appropriate lenses to collimate the beam of diode laser devices with fill factor greater than 50 %. In this case the beam collimation is problematic because the array of

slow axis collimation (SAC) lenses should be very close to the source, due to the short distance between adjacent emitters that causes a "fast" divergence of the slow axis in short distances. Consequently, there would be not space to include a fast axis collimation (FAC) lens that normally comes first [8-9]. In this paper, the technical goal is to develop a laser source to illuminate a target at high intensity with a near-square pattern. The approach is to use a high-power DLB with fill factor of 76 % (emitter width and pitch of 190 µm and 250 µm, respectively), taking into account a realistic model of Jenoptik (JDL-BAB-75-37-940-TE-300-1.5) with 37 emitters and radiating in the near-infrared (NIR) at the central wavelength of 940 nm, suitable for optoacoustic imaging [10]. We propose a customized lens design for this DLB. Collimating and beam focusing lenses have been designed in Zemax environment to reduce the beam size of the abovementioned DLB. In this case, the collimating lenses have not been positioned close to the source but at a certain distance that allows the beam symmetrization between the two axes and the



collimation. More specifically, cylindrical FAC and SAC lenses have been positioned at 12 mm and 23 mm from the DLB, respectively. In such a way, the beam is symmetrized and collimated at the same time. As a result, the beam observed on a detector plane (at 40 mm from the source) shows a semisquare shape (~ 12.35 mm x 11.62 mm) that facilitates its handling in a successive stage. Then, a second pair of crossed cylindrical lenses has been designed to reduce the beam size. Successively, another pair of cylindrical lenses (one plano-concave and the other one plano-convex) is used to reshape the beam in a smaller spot with size of ~ 3.7 mm x 3.7 mm (at $1/e^2$) and intensity of ~ 3.2 kW/cm². Due to the large number of emitters, the beam spot could not be reduced more in the slow axis. Basically, the

latter lens pair has been designed to achieve a square spot for optoacoustic applications in which a homogeneous beam profile is required for uniform light focusing on an absorbing target.

2. Results

The beam collimation is showed in Figure 1 and the optical elements are arranged following the order of the abovementioned description. In Table 1, the main characteristics of the DLB are reported. The high number of emitters (37) of this bar is responsible for such high output peak power (300 W) but goes to the detriment of the beam quality, due to a higher beam parameter product (*BPP*). The characteristics of the collimating lenses are listed in Table 2.



Figure 1. Simulation scheme of the optical system collimating a DLB from Jenoptik (JDL-BAB-75-37-940-TE-300-1.5) with 37 emitters and 76 % fill factor: lateral view of a) fast axis and b) slow axis. The emitter width and pitch are 190 μ m and 250 μ m, respectively. The image shows very good collimation in both axes. Actually, the beam is not collimated but keeps a semi-square pattern for a certain distance after the SAC lens (i.e. ~ 88 mm).

Characteristic	Value	
Central wavelength	940 nm	
Regime	QCW*	
Output peak power	300 W	
Fast axis beam divergence (1/e ²)	47.5 ± 1.5°	
Slow axis beam divergence (1/e ²)	10 ± 1°	
Single emitter contact width	190 µm	
Emitter pitch	250 µm	
Number of emitters	37	
Fill factor	76%	



The beam-parameter product (*BPP*) is necessary to estimate the beam quality in both fast and slow axes. In fast axis, it is defined as the waist radius w_{0x} (i.e. the half of the vertical size in fast axis) multiplied by the half angle divergence $\theta_{\perp half}$ of the beam along the fast axis. Instead, in the slow axis it corresponds to the waist radius w_{0y} (which in our case corresponds to the half of the emitter width in slow axis (see Table 1)) multiplied by the half angle divergence $\theta_{//half}$ of the beam along the slow axis and the number of emitters, normalized to the bar fill factor. Hence, the *BPP*_s in fast axis and slow axis (*BPP*_x and *BPP*_y) are respectively expressed by:

$$BPP_x = w_{0x} \times \theta_{\perp half} , \qquad (1)$$

$$BPP_{y} = \frac{w_{0y} \times \theta_{//half} \times \text{number of emitters}}{\text{bar fill factor}}$$
(2)

where the bar fill factor is normally expressed in % and is the ratio between the emitter width and the emitter pitch (Table 1). In order to achieve the necessary beam quality for an efficient fiber coupling, the *BPP* ratio (*BPP_y/BPP_x*) should be made as close as possible to 1 by means of beam shaping lenses. Assuming a vertical size of 2 µm (namely $w_{0x} = 1$ µm) for each emitter, at the output of the DLB, the *BPP_s* in fast axis (*BPP_x*) and slow axis (*BPP_y*) are respectively:

$$BPP_x = 1 \ \mu m \ x \ 23.75^{\circ} \approx 0.41 \ \mu m \cdot rad,$$
 (3)

$$BPP_{y} = \frac{95 \,\mu\text{m.x 5}^{\circ} \,x\,37 \text{ emitters}}{\text{fill factor}} \approx 403.607 \,\mu\text{m.rad}, \qquad (4)$$

Hence, from Eqs. (3) and (4) it can be derived that:

$$\frac{BPP_y}{BPP_x} \approx 984.4 \tag{5}$$

that will be significantly reduced after collimation. Figure 2 shows more in detail the DLB composed of an array of emitters.

Component	FAC lens	SAC lens		
Material	N-LAF21	N-LAF21		
Height (mm)	16	16		
Thickness (mm)	4.5	3.8		
Length (mm)	16	16		
Radii of curvature (mm)	Infinite/ 11.1	Infinite/ 70		
Conic constant	-1	-1		
Distance from DLB (mm)	12	23		

 Table 2. Characteristics of the collimating lenses.

It can be noticed how much is short the spacing between adjacent emitters. Even though the slow axis divergence is little $(10 \pm 1^{\circ})$, the rays of each emitter intersect those of the adjacent emitters at very close distances from the source. The beam profile simulated at 40 mm from the source is represented in Figs. 3 and 4 as graph and image,

respectively. Both the FAC and SAC lenses are plano-convex and their curvature is in the front face of the lenses. As a result, the collimated beam takes a semi-square shape (~12.35 mm x 11.62mm at $1/e^2$ of the peak) that is easier to focus in a successive stage. The detector image shows that the major contribution of power is in the central part of the



beam, following the principle of Gaussian beam. In a second step we show the beam focusing in a square spot. Normally, in optoacoustic applications is required to focus the beam in a spot to illuminate small regions of biological tissues for in-depth imaging with high resolution. In this regard, we reduced the beam size in a square spot of ~ 3.7 mm x 3.7 mm (at $1/e^2$) using two additional pairs of cylindrical lenses. The characteristics of these lenses are listed in Table 3 and they are labeled with their numeration. Figure 5 shows the whole lens system including the focusing lenses to reduce the beam spot size. The square spot is captured at a distance of 75 mm from the source (Figure 6). The spot size is a square with size of ~ 3.7 mm x 3.7 mm and intensity of ~ 3.2 kW/cm² (Figs. 6 and 7). At this stage, the values for the two BPPs have now been nearly symmetrized. The BPPv has been reduced to 403.607 µm·rad /37 ≈ 10.908 µm·rad, while BPP_x has increased to 0.41 μ m·rad x 37 \approx 15.17 μ m·rad. In such a way, it can be derived that:

$$\frac{BPP_x}{BPP_y} \approx 1.39\tag{6}$$

which corresponds to a BPP reduction factor of ~708. Then, the footprint on the target is reduced by a linear factor of ~37, and the intensity on target is increased by a factor of $\sim 37^2 = 1369$. The intensity on the detector is limited by the inability to reduce the square footprint below 37 mm in the slow axis. This depends directly on the large value of BPP_{v} at the output of the DLB. Considering a typical pulse width of 200 ns in optoacoustic applications [11], the intensity of ~3.2 kW/cm² achieved with the proposed design corresponds to 0.64 mJ/cm², which is compatible with the limit of maximum energy density applicable to a biological tissue, which is 20 mJ/cm² following ANSI safety standard. The large number of the emitters, combined with the high fill factor of this DLB, does not allow the beam focusing in a smaller spot that is required in optoacoustic endoscopy using coupling into optical fibers (< 600 µm), but consents other optoacoustic applications in free space.





Figure 2. DLB array of 37 emitters at close distance: a) size of the whole array, b) size of each emitter and pitch.

Figure 3. Profile of the collimated beam in: a) fast axis and b) slow axis. The beam size is ~ 12.35 mm x 11.62 mm at $1/e^2$.





Figure 4. Image of the beam profile observed on a detector located after collimating lenses.



Figure 5. Whole lens system to reduce the size of the beam spot: a) lateral view, b) top view. At longer distances (i.e. ~ 8 mm from the last focusing lens), the beam divergence would be larger in the slow axis due to the large number of emitters.

Component	Focusing lens 1	Focusing lens 2	Focusing lens 3	Focusing lens 4
Material	S-LAH64	S-LAH64	S-TIH53	S-TIH53
Height (mm)	16	16	5	5
Thickness (mm)	5	7	1.5	3
Length (mm)	16	16	10	10
Radii of curvature (mm)	-21.984/ Infinite	-21.984/ Infinite	Infinite/ -7.5	Infinite/ 10
Conic constant	0	0	0	0
Distance from DLB (mm)	33	41	56.3	64

Table 3. Characteristics of each focusing lens for beam size reduction.





Figure 6. Image of the beam focused observed on a detector.



Figure 7. Beam profile of the focused beam in: a) fast axis and b) slow axis. The beam size is ~ $3.7 \times 3.7 \text{ mm}$ at $1/e^2$.

Conclusions

In summary, we have presented the design of a customized lens system to reduce the beam size of DLBs with fill factor greater than 50 %. Our results demonstrate a good collimation in both fast and slow axis and a focusing in a small spot. This work opens the opportunity of development of the proposed lenses for beam focusing of DLBs with high fill factor. Their characteristics of high brilliance and high optical power are particularly useful for penetrating in depth into biological tissues. Future work should be addressed to the implementation of the lens system proposed in this paper.

In this way, the optoacoustic imaging at 940 nm of some chromophores like lipids and hemoglobin would get benefit from these DLBs.

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Declaration of interest

The authors have no financial interests in the manuscript. There are no potential conflicts of interest to declare.



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